

ACTA TECHNICA CORVINIENSIS - Bulletin of Engineering Tome VI (Year 2013) - FASCICULE 2 [April-June] ISSN 2067-3809



^{1.} Saša RANĐELOVIĆ, ^{2.} Dragan MIŠIĆ, ^{3.} Miroslav TRAJANOVIĆ, ^{4.} Nikola VITKOVIĆ, ^{5.} Marko VESELINOVIĆ

CUSTOMIZATION OF ORTHOPEDIC INTERNAL FIXATOR

^{1-5.} University of Niš, Faculty of Mechanical Engineering, SERBIA

ABSTRACT: Customization and adjustment of medical devices and elements for external and internal fixation is a major challenge in modern orthopedic surgery. As a result a large number of minor and serious illnesses and injuries, congenital disorders, or more often emerging with a large number of anatomical requirements, impose the various technical requirements to be met with one, two or more orthopedic element. Modern lifestyle and pace of today's man activities carries great dangers and risks. At a given moment and inception health condition, expert team will usually need to react very fast, high quality and tested to achieve the desired effect. Since this is a human health or the disruption and damage to his bones and joint system, orthopedic devices and components shall as far as possible be adapted to meet the technical requirements and standards set and standards set. KEYWORDS: Orthopedic fixation, production, orthopedic material, FEM analysis

Type of injury or disease stage directly determines the medical diagnosis and therefore the medical procedure to be undertaken. In real conditions, in addition to the usual procedures, medical equipment and supplies, sometimes is not enough to use standard components of the implant because of unusual anatomy or potential risk of postoperative complications, such as aseptic weakening. The usual reason for aseptic weakening is the uneven distribution of mechanical stress to the bone volume and the irregular 3D surfaces of bones. This problem can be solved using customization implant design, customized to the specific characteristics of the patient's anatomy.

DESIGN AND MANUFACTURE OF FIXATIONS

Tibia is situated at the medial side of the leg and composed of middle part (tibial shaft - body) and two extremities: proximal part and distal part. Proximally the tibia has a broad articular surface which articulates with the femur [1].

Tibial plateau (proximal/superior articular surface) fractures are typically complex fractures associated with poor outcomes and a high rate of complications and their treatment remains problematic [2]. Fixation method with Mitkovic's internal fixator type TPL(tibia-plato-lateral) is possible treatment solution for such kind of injuries.

Fixator needs to fit onto the proximal lateral tibia surface. Therefore, in order to obtain the best possible fit, anatomically pre-contouring Mitkovic's TPL fixator is well solution. Customization can be undertaken by changing values of dimensions of geometrical entities for previously created 3D fixator model. New values can be obtained from certain radiology image of the bone [3].

Research and development for customization production of orthopedic implants is typically related to direct manufacturing technologies [4,5]. New equipment for the rapid production of prototypes (rapid-manufacturing) allows much greater efficiency in small series or individual production.



Figure 1. Lower Extremities, 1. Femur, 2. Tibia, 3. Fibula [3]

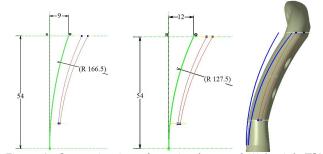


Figure 2. Customization of proximal part of Mitkovic's TPL fixator in order to achieve accurate fixation for specific patient's tibia bone

The latest methods used for the direct production of high strength materials such as titanium, is the melting of the electron beam (electron-beam melting - *EBM*).



Figure 3. EBM process

The application contains a conventional treatment methods that allow a larger series of products with a smaller adjustment fixators for a given concrete conditions.

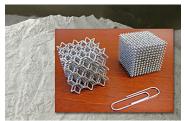


Figure 4. Additive technology

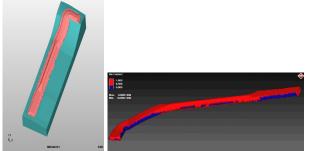


Figure 5. Lower tool for hot forging technology and finished part for orthopedic fixation

Additive manufacturing, sometimes called "3D printing," is a group of new technologies that build up objects by adding materials, usually by laying down many thin layers. It is so called to distinguish it from traditional machining that creates objects by cutting material away.

Processes of metal forming, both cold and hot working offer technology solutions and still have not overcome the majority of patients. These technologies covered most medical cases in the external and internal fixation. This results in greater savings and necessary for customization products.

Orthopedic implants can be very complex, customized products to be produced, based on the above information as soon as possible [6]. Key factors of production for customization orthopedic implants are the level of customization of the final product and delivery time. A higher level of customization reduces the duration of the operation and increases the reliability of future implants. Also, reducing the present risks from possible complications.

The general approach in developing the technology of manufacturing companies is to optimize the design of their products according to criteria of simplicity and cost, while adapting their processes mainly for large series production. This is the main reason why they are not able to produce small batches or individual products in an efficient manner. In the traditional sense, the processes for the production of customization implants include a large number of analysis and decision making, such as interpretation and analysis of CT (Computed Tomography) scans,

analysis of wax prototypes, mechanical analysis, information gathering and permits, etc. Lack of efficiency to adapt their traditional workflow activities becomes even more critical when companies have to hire suppliers of various parts, components or services.

The fact is that this process involves intensive communication, a number of consultations between the various experts which discuss of the functional (medical), mechanical, organizational, and other perspectives on the process of customized production.



Figure 6. Distal-lateral, proximal-lateral and lateral plate

process models represent different are informations which describing orthopedic implants. provide aim to relevant knowledge representation and reasoning in decision making regarding treatment and preoperative planning, and configuration of the virtual enterprise, planning, technology and business process management. For example a generic 3D parametric model selected human bone, can be generated by the available tools and features in one of the 3D modeler. Although a lot of complex surfaces and volumes require a combination of very powerful software options, it is a good way to make a multi-functional model. This will be fully covered by the technical documentation and important details, model development, model analysis and simulation of stress and many other sensitive issues. Attempt to irregular and complex surface and volume dependent on parameter representing mathematical functions relationships only slightly speeds up the design. Time to get models with high probability, at a later stage will not provide an opportunity for a complete analysis.



Figure 7. Front and medial plate for lowerleg fixation



Figure 8. Distal-periarticular plate

Implants are usually made from scaffold, fixing (used for heavier loaded bones) and bio-degradable materials for osteo-fixation. These models are generated based on data obtained from CT scans and are essential for digital reconstruction of traumatized bone. Then, based on this model, it is possible designing the scaffold, which replaces the missing part bone. Simulation models allow the prediction and optimization of mechanical behavior

of implants under realistic load conditions, using FEM methods (Finite Element Analysis - FEA).

SELECTION OF MATERIALS FOR ORTHOPEDIC FIXATORS

Modern medical implants are products which have to satisfy strict standard requirements regarding materials, machining technologies and their functionality. They could be used in almost every organ of the human body. Ideally they should have biomechanical properties comparable to those of autogenous tissues without any adverse effects. The principal requirements of all medical orthopedic implants are corrosion resistance, biocompatibility, bioadhesion, biofunctionality, machinability and availability.

To fulfill these requirements most of the tests are directed into the study extracts from the material, offering screens for genotoxicity, carcinogenicity, reproductive toxicity, cytotoxicity, irritation, sensitivity and sterilization agent residues [7].



Figure 9. T- plate, proximal

Modern medical implants are regulated and classified in order to ensure safety and effectiveness to the patient. One of the most favorable biomaterial used for biomedical applications is titanium alloy Ti6Al4V due to its combination of the most desirable characteristics including immunity to corrosion, biocompatibility, shear strength, density and osteo-integration. The excellent chemical and corrosion resistance of titanium is caused by the chemical stability of its solid oxide surface layer to a depth of 10 nm. Under in-vivo conditions the titanium oxide (TiO₂) is the only stable reaction product whose surface acts as catalyst for a number of chemical reactions, [8].

The biggest risk wear contact between implant and the bone surface, which largely depends on the type of implant materials [9].

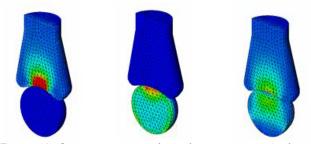


Figure 10. Contact stress analysis, bone vs. ceramic, bone vs. polyethylene and bone vs. pyrocarbon

In the case of ceramics with extremely high elastic modulus (407 GPa), there is almost no distortion, and it is a solid contact with the implant that does not respond to the effect of mechanical stress or mechanical force causes a large increase in internal stresses in the bone itself. Polyethylene in contact with the bone mass has completely different characteristics. Its much lower elastic modulus (1 GPa) suggests that the entire burden is transferred to

the established contact implant and the bone implant produced a disproportionate strain which is not permissible. It is clear that pure pirokarbon, when such an analysis, show the best mechanical properties, that is closest to the behavior of human bone mass [8,9,10].

Table 1. Biocompatibility and Bioelasticity Facts

rable it broompatibility and brookasticity racts							
	Silicone	auog	Pure Pyro- carbon	Titaniu m (TA6V)	Cobalt Chrome (CrCo)	Ceramic (Alumin a)	
E (GPa)	0.0004	15 - 20	20 - 25	110	200 - 240	407	
Density (g.cm ⁻³)	1.1	2.0	1.7 - 2.0	4.5	8.3 - 9.2	3.5	

The basic idea in the development of new alloys for medical applications, therefore, is to replace aluminum and vanadium with niobium, tantalum and zirconium. In order to thus avoid the negative features are now widely applied to the Ti-6Al-4V alloy, as shown that the toxicity of these elements is extremely low.

The alloy Ti-13Nb-13Zr, developed in the United States, shows remarkable properties. This is the type of B titanium alloys and is characterized by low values of elastic modulus and strength significantly improved in comparison to commercial Ti-6Al-4V alloy, which is extremely interesting for applications in biomedical engineering [10].

The relatively low hardness of titanium alloys, however, affect their poor wear resistance, and these alloys without additional surface treatment such as ion implementation, can not be used for the preparation of joint surfaces.

THE LEVEL OF CUSTOMIZATION AND COMPLIANCE WITH STANDARDS

Experience shows that any impromptu or untested solutions very quickly cause unwanted effects and consequences that are difficult or impossible to correct. For these reasons, the entire field of medicine, and orthopedic and reconstructive surgery requires the application of certain standards and guidelines will be a limit to customization and extensions.

The ISO-13485 is an international quality management system (QMS) standard defined for the medical device industry. It is therefore important for manufacturers of equipment, apparatus (accessories) and semiconductor devices used in medical electronics to get certified to the ISO-13485 in order to secure and maintain global business. Created by the International Organization for Standardization (ISO), the ISO-13485:2003 borrowed the structure of the ISO-9001:2000.



Figure 11. Distal, distal medial and proxsimal-medial plate

2013. Fascicule 2 [April–June]

The benefits of registration to ISO-13485 include: 1) international recognition of compliance with the FDA Quality System Regulations and unique medical industry standards, facilitating global business; 2) a more efficient, cost-effective, and stable organization; 3) improved process, product, and service quality; and 4) better documentation of existing processes.

ISO-13485:2003 basically consists of: 1) certain ISOrequirements and 2) newly defined requirements catering specifically to the medical device industry. As such, ISO-13485 differs from ISO-9001 in certain ways, modifying or even excluding some of the latest requirements. For instance, the ISO-13485 excludes the ISO-9001's requirements related to continual improvement because most medical device regulations require organizations to maintain their quality management systems, and not to improve them. Thus, while ISO-9001 emphasizes the importance of improving quality systems, ISO-13485 emphasizes the importance of maintaining them. ISO-9001 customer satisfaction requirements were also excluded because some of the committee members who worked on ISO-13485 found them to be too subjective.

Some key points adopted by the ISO-13485 include: 1) focus on meeting regulatory requirements; 2) focus on meeting customer requirements; 3) use of a 'process' approach; 4) maintenance of the effectiveness of quality management systems; and 5) maintenance of procedural documentation.

As mentioned, the ISO-13485 has special requirements that are not covered by ISO-9001:2000. These special requirements include both documentation and system/process requirements that cater to the medical device industry.

Aside from regulation-required documents, additional documentations required by ISO-13485 include those pertaining to: 1) responsibilities and authorities; 2) training procedures; 3) health, and clothing; cleanliness, 6) environmental conditions; 7) control of contaminated products; 8) risk management; 9) customer requirements; 10) design and development; 11) purchasing control, including purchase traceability and verification; 12) reference materials; 13) labeling and packaging; 14) installation and verification; 15) sterilization process validation; 16) preservation of product (including shelf life); and 17) measurement and monitoring.

Special system / process requirements of the ISO-13485 include: 1) risk management systems; 2) clinical evaluations and trials; 3) product cleanliness and contamination controls; 4) requirements for implantable devices; 5) proper communication of advisory notices; and 6) additional research and development requirements.

CONCLUSIONS

Extensively investigations and the facts point to the possibilities and advantages of new technologies in the field of orthopedic surgery and in other medical disciplines.

If the problem considered multidisciplinary, using new technologies and higher degree of customization with good knowledge of the properties of new materials and alloys, patients get a much better chance in their fight for a healthy and normal life. It is certain that medicine retains a leading and crucial role in such a complex process, along with the fact that it must always be ready to accept the latest developments in related disciplines that offer its latest solutions and results.

ACKNOWLEDGEMENT

This paper is part of project III41017 Virtual human osteoarticular system and its application in preclinical and clinical practice, funded by the Ministry of Education and Science of Republic of Serbia.

REFERENCES

- [1.] P. Brown, "The online skeleton", from http://www-personal.une.edu.au/~pbrown3/oskel.html, accessed on 2012-10-15.
- [2.] N. Russell, P. Tamblyn, R. Jaarsma, "Tibial plateau fractures treated with plate fixation: to lock or not to lock", Eur J Orthop Surg Traumatol, 19, 2009, pp. 75-82.
- [3.] T. B. Moeller, E. Reif, "Pocket Atlas of Radiographic Anatomy", Second edition, Thieme, Stuttgart · New York, 2000, pp. 156.
- [4.] MW. Chapman. "Principles-of-internal and external fixation", Chapman's orthopaedic surgery. 3rd ed. Lippincott Williams and Wilkins; 2001.
- [5.] R. Thull, D. Grant, "Physical and Chemical Vapor Deposition and Plasma-assisted Techniques for Coating Titanium", In Titanium in Medicine, Brunette D.M., Tengvall P., Textor M., Thomsen P. (eds.), Springer-Verlang Berlin Heidelberg, 2001. pp. 284-335.
- [6.] P. Tengvall, I. Lundstrom, "Physico-chemical considerations of titanium as a biomaterial", Clin. Materials 9, 1992. pp.115-134.
- [7.] F. Wataria, A. Yokoyamaa, M. Omorib, T. Hiraic, H. Kondoa, M. Uoa, T. Kawasakia, "Biocompatibility of materials and development to functionally graded implant for bio-medical application", Composites Science and Technology 64, 2004, pp. 893-908.
- [8.] M. Viceconti, M. Casali, B. Massari, L. Cristofolini, S. Bassinit, A. Toni, "The 'standardized femur program' proposal for a reference geometry to be used for the creation of finite element models of the femur", J. Biomech. 1996; 29(9):1241.
- [9.] Ž. Stepanović, M. Živković, S. Vulović, Lj. Aćimović, B. Ristić, A. Matić, Z. Grujović, "Visoka, otvorena, klinasta osteotomija tibije: analiza pet modaliteta unutrašnje fiksacije metodom konačnih elemenata", Vojnosanitetski pregled, vol 68, br.10, 2011, pp. 867-871.
- [10.] N. Vitković, J. Milovanović, M. Trajanović, N. Korunović, M. Stojković, M. Manić, "Methods for creating geometrical model of femur anatomical axis" 34th International Conference on Production Engineering, ICPE 2011, September 28th 30th, 2011, Nis, Serbia

ACTA TECHNICA CORVINIENSIS – BULLETIN of ENGINEERING







ISSN: 2067-3809 [CD-Rom, online]

copyright © UNIVERSITY POLITEHNICA TIMISOARA, FACULTY OF ENGINEERING HUNEDOARA, 5, REVOLUTIEI, 331128, HUNEDOARA, ROMANIA http://acta.fih.upt.ro